



ORAL PRESENTATION

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Quantitative free-breathing 3T T_2 -mapping of the heart designed for longitudinal studies

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Background

Recently, T_2 -weighted MRI for the characterization of edema after myocardial infarction has attracted considerable attention (Friedrich, *NatRevCardiol*2010). Furthermore, the recently proposed combination of bSSFP imaging and T_2 Prep for T_2 -mapping at 1.5T has enabled a rapid quantitative cardiac T_2 estimation (Huang et al., *MRM*2007). However, the accuracy of this method may still be limited due to the complex T_2/T_1 signal weighting. Especially for longitudinal studies designed for monitoring and/or guiding therapy, accurate and reproducible T_2 measurements will be critical. A novel quantitative 3T T_2 -mapping protocol was therefore developed and tested in both healthy volunteers and patients.

Methods

An adiabatic T_2 prep with 3 incremental TE values, affine coregistration, a navigator and 2D radial gradient echo imaging were combined for free-breathing T_2 -mapping at 3T with a spatial resolution of 1.25mm. Bloch equation simulations of this sequence were used to optimize scan parameters and to determine an empirical equation that compensates for T_1 relaxation and which returns the "true" T_2 . The T_2 -mapping sequence and empirical equation were then validated in a series of 15 phantoms in which the true T_2 was determined with a 9-TE spin-echo sequence. Next, the myocardial short axis T_2 of 8 healthy volunteers was mapped in two different scan sessions while a reference phantom ($T_2=43.1 \pm 0.7$ ms) was placed next to the thorax. The average myocardial T_2 for both sessions was computed with and without correction with the "true" reference phantom

T_2 . Finally, this validated protocol was used in 5 patients in the subacute phase after revascularization of acute ST-elevation myocardial infarctions and compared to T_2 -weighted TSE imaging.

Results

As a result of both the simulations and phantom scans, optimized sequence parameters included: $TE_{T_2\text{prep}}=60/30/0$ ms, $T_{RR}=3$ heartbeats, $TR/TE=5.3/2.4$ ms. The empirical equation to determine T_2 was $S=S_0[\exp(-TE_{T_2\text{prep}}/T_2)+0.06]$, where S and S_0 are the measured and steady-state signal (Fig. 1a). Scans of the phantoms with known T_2 confirmed a $12 \pm 2\%$ ($p < 0.001$) improvement in T_2 estimation with the empirical equation as compared to the standard T_2 decay measurements (Fig. 1b). The myocardial T_2 in the volunteers was homogeneous (42 ± 5 ms over all volunteers) and on average showed a $5 \pm 2\%$ difference between the two scan sessions. When compensated with the T_2 from the reference phantom, this difference decreased to $2 \pm 1\%$ ($p=0.02$). In all patients, T_2 maps could successfully be obtained and a clear demarcation of zones with elevated T_2 values was consistent with the findings on T_2 -weighted MRI and X-ray coronary angiography as shown in the example in Fig. 2.

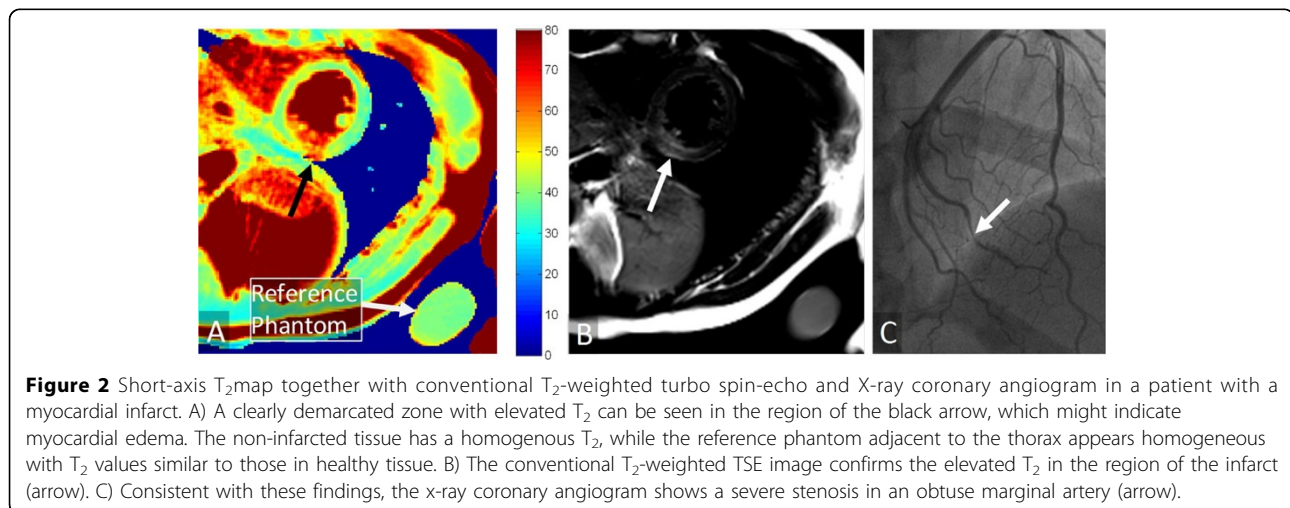
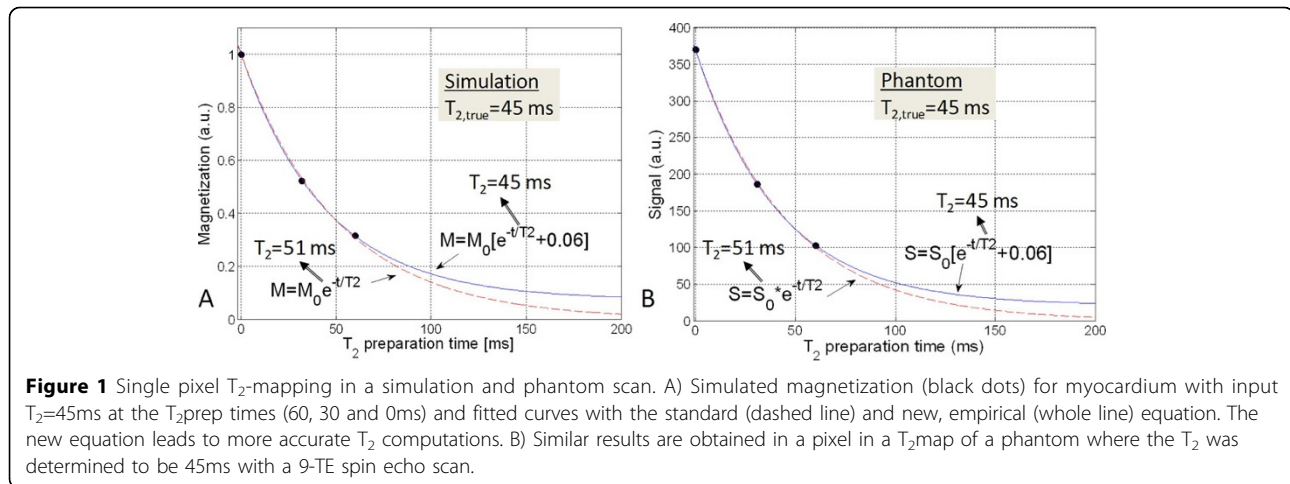
Conclusions

The methodology presented in this study enables robust and accurate cardiac T_2 -mapping at 3T, while the addition of a reference phantom improves reproducibility. Therefore, it may be well-suited for longitudinal studies in patients with ischemic heart disease.

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