### **ORAL PRESENTATION**

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# Quantitative free-breathing 3T T<sub>2</sub>-mapping of the heart designed for longitudinal studies

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#### **Background**

Recently,  $T_2$ -weighted MRI for the characterization of edema after myocardial infarction has attracted considerable attention (Friedrich, NatRevCardiol2010). Furthermore, the recently proposed combination of bSSFP imaging and  $T_2$ Prep for  $T_2$ -mapping at 1.5T has enabled a rapid quantitative cardiac  $T_2$  estimation (Huang et al., MRM2007). However, the accuracy of this method may still be limited due to the complex  $T_2/T_1$  signal weighting. Especially for longitudinal studies designed for monitoring and/or guiding therapy, accurate and reproducible  $T_2$  measurements will be critical. A novel quantitative 3T  $T_2$ -mapping protocol was therefore developed and tested in both healthy volunteers and patients.

#### **Methods**

An adiabatic  $T_2$  prep with 3 incremental TE values, affine coregistration, a navigator and 2D radial gradient echo imaging were combined for free-breathing T2-mapping at 3T with a spatial resolution of 1.25mm. Bloch equation simulations of this sequence were used to optimize scan parameters and to determine an empirical equation that compensates for T<sub>1</sub> relaxation and which returns the "true" T<sub>2</sub>. The T<sub>2</sub>-mapping sequence and empirical equation were then validated in a series of 15 phantoms in which the true T2 was determined with a 9-TE spin-echo sequence. Next, the myocardial short axis T2 of 8 healthy volunteers was mapped in two different scan sessions while a reference phantom (T<sub>2</sub>=43.1 ±0.7ms) was placed next to the thorax. The average myocardial T<sub>2</sub> for both sessions was computed with and without correction with the "true" reference phantom  $T_2$ . Finally, this validated protocol was used in 5 patients in the subacute phase after revascularization of acute ST-elevation myocardial infarctions and compared to  $T_2$ -weighted TSE imaging.

#### Results

As a result of both the simulations and phantom scans, optimized sequence parameters included: TE<sub>T2prep</sub>=60/ 30/0ms,  $T_{RR}=3$  heartbeats, TR/TE=5.3/2.4ms. The empirical equation to determine T<sub>2</sub> was S=S0[exp  $(-TE_{T2prep}/T_2)+0.06$ ], where S and S0 are the measured and steady-state signal (Fig. 1a). Scans of the phantoms with known T2 confirmed a 12±2%(p<0.001) improvement in T<sub>2</sub> estimation with the empirical equation as compared to the standard T2 decay measurements (Fig. 1b). The myocardial  $T_2$  in the volunteers was homogeneous (42±5ms over all volunteers) and on average showed a 5±2% difference between the two scan sessions. When compensated with the T<sub>2</sub> from the reference phantom, this difference decreased to 2±1% (p=0.02). In all patients, T<sub>2</sub>maps could successfully be obtained and a clear demarcation of zones with elevated T<sub>2</sub> values was consistent with the findings on T<sub>2</sub>weighted MRI and X-ray coronary angiography as shown in the example in Fig. 2.

#### Conclusions

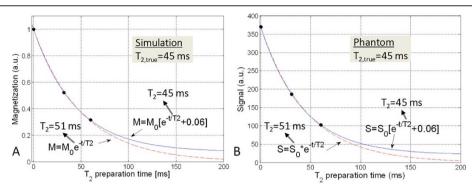
The methodology presented in this study enables robust and accurate cardiac  $T_2$ -mapping at 3T, while the addition of a reference phantom improves reproducibility. Therefore, it may be well-suited for longitudinal studies in patients with ischemic heart disease.

#### **Funding**

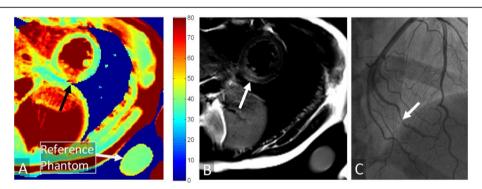
N/A.

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**Figure 1** Single pixel  $T_2$ -mapping in a simulation and phantom scan. A) Simulated magnetization (black dots) for myocardium with input  $T_2$ =45ms at the  $T_2$ prep times (60, 30 and 0ms) and fitted curves with the standard (dashed line) and new, empirical (whole line) equation. The new equation leads to more accurate  $T_2$  computations. B) Similar results are obtained in a pixel in a  $T_2$ map of a phantom where the  $T_2$  was determined to be 45ms with a 9-TE spin echo scan.



**Figure 2** Short-axis  $T_2$ map together with conventional  $T_2$ -weighted turbo spin-echo and X-ray coronary angiogram in a patient with a myocardial infarct. A) A clearly demarcated zone with elevated  $T_2$  can be seen in the region of the black arrow, which might indicate myocardial edema. The non-infarcted tissue has a homogenous  $T_2$ , while the reference phantom adjacent to the thorax appears homogeneous with  $T_2$  values similar to those in healthy tissue. B) The conventional  $T_2$ -weighted TSE image confirms the elevated  $T_2$  in the region of the infarct (arrow). C) Consistent with these findings, the x-ray coronary angiogram shows a severe stenosis in an obtuse marginal artery (arrow).

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