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Assessment of 3D velocity vector fields and turbulent kinetic energy in a realistic aortic phantom using multi-point variable-density velocity encoding

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From 15th Annual SCMR Scientific Sessions Orlando, FL, USA. 2-5 February 2012

Summary

A multi-point velocity encoding approach for the assessment of velocity vector fields and TKE is shown in this work. The method is applied in an aortic arch phantom under different flow conditions.

Background

Three-dimensional Phase Contrast (PC) MRI has emerged as a promising non-invasive acquisition technique for assessing velocity vector fields of blood flow [1]. To address the limited sensitivity when velocities are much lower than the encoding velocity v_{enc}, three-point acquisition methods with a high v_{enc} and a low v_{enc} acquisition to unwrap the low $v_{\text{enc}}\ scan$ may be employed [2]. However, by using the high v_{enc} data only to control phase unaliasing the approaches are not signal-to-noise ratio (SNR) efficient. This fact becomes relevant in particular when incorporating data undersampling techniques to shorten the long scan times associated with 3D PC-MRI. Accordingly, SNR optimality of encoding and decoding is desired. To this end Bayes' approaches have been proposed and adapted to PC-MRI [3,4].

In the present work the feasibility of velocity vector field and turbulent kinetic energy (TKE) mapping based on multi-point variable-density velocity encoding with spatiotemporal undersampling is demonstrated on a realistic aortic phantom [5].

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An elastic cast of an aortic arch equipped with a mechanical aortic valve (St. Jude Medical Inc., St. Paul, MN, USA) was set up in a pulsatile flow conduit and measured using a velocity encoded, cardiac triggered 3D gradient echo sequence on a 3T Philips Achieva System (Philips Healthcare, Best, The Netherlands). Within a scan time of 33 min, 5 velocity encodings according to $v_{\rm enc}$ = [200, 100, 50, 28, 20] cm/s in each spatial direction plus a non-encoded reference segment were acquired (Fig 1. red dots) with 5x k-t undersampling and 11x6 training profiles with a temporal resolution of 46 ms. Velocities and TKE values [5] were computed using Bayesian parameter estimation [6]. In a second experiment, one leaflet of the valve was fixed in order to simulate a stenotic valve.

Results

Mean TKE values in the ascending aorta were found to be about 4 times higher for the stenosed valve experiment compared to a normal heart valve. The jet of high velocities up to 100 cm/s is surrounded by increased TKE areas with TKE values > 50 J/m³ as it is shown in Fig. 2 b) & d).

Conclusions

The presented work shows the assessment of velocity vector fields and TKE in a realistic aortic phantom. Using the identical setup comparison of TKE values to data from Particle Tracking Velocimetry (PTV) is possible hence permitting assessment relative to a method of reference for measuring fluctuating velocities at very high temporal resolution.



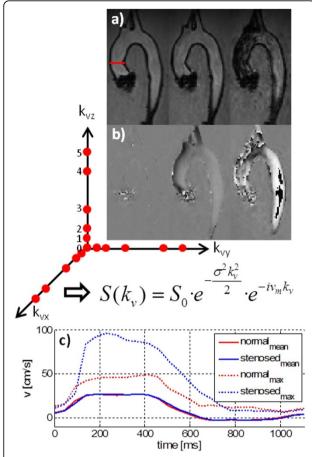


Figure 1 Magnitude (a) and phase (b) images reconstructed from velocity encodes marked in red with 0, 2 and 5 from left to right. The mean velocities v_m and TKE are estimated voxelwise. Throughplane velocity profiles measured at the red contour in (a) are shown for the normal and stenosed valve in (c).

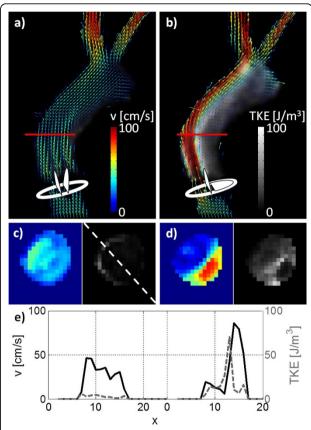


Figure 2 Velocity vector fields and TKE values are shown for t = 322 ms for an axial slice through the normal and stenosed valve (a-b). Absolute velocity and TKE values along profiles marked in (c-d) show an inhomogeneous velocity distribution in the stenosed experiment with high TKE values in the separation plane.

Funding

SNF K-32K1 120531/1.

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Published: 1 February 2012

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doi:10.1186/1532-429X-14-S1-W50

Cite this article as: Knobloch *et al.*: Assessment of 3D velocity vector fields and turbulent kinetic energy in a realistic aortic phantom using multi-point variable-density velocity encoding. *Journal of Cardiovascular Magnetic Resonance* 2012 14(Suppl 1):W50.

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