

**WORKSHOP PRESENTATION**

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# A subspace approach to blind coil sensitivity estimation in parallel MRI

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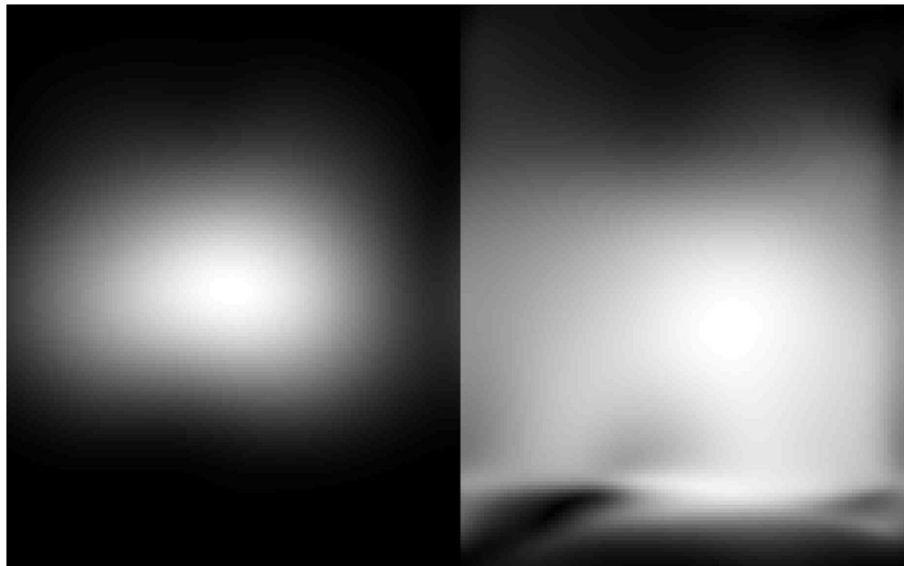
## Background

In parallel MRI, subsampled k-space data are simultaneously collected by multiple coils. Each coil introduces a sensitivity map (CSM) that is multiplied pointwise with the single image to be reconstructed. In ESPIRiT [1], for each pixel location in each coil, an eigen-decomposition is applied to small matrices to obtain CSMs. However, this approach can be time-consuming for larger imaging problems. Here, we exploit smoothness of the coil sensitivities in the image domain to model them as small finite impulse response (FIR) filters in

k-space as in PRUNO [2]. Since pointwise-multiplication in image domain corresponds to convolution in k-space, parallel MRI problem can be expressed as a blind image deconvolution problem; consequently, a subspace approach [3] can be used to estimate the k-space coefficients of the CSMs.

## Methods

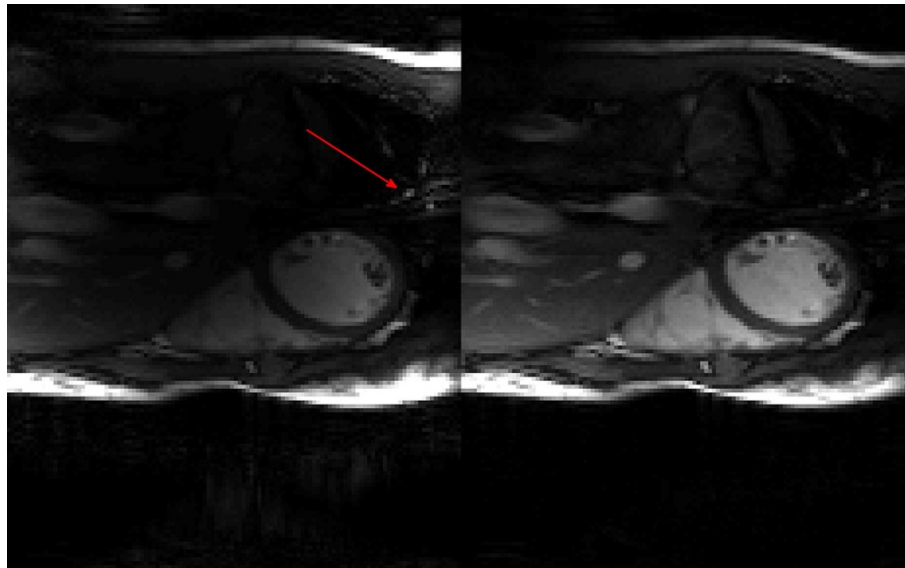
If  $y_i$ ,  $x$  and  $h_i$  represent fully sampled k-space data, true image, and k-space coefficients of the  $i^{\text{th}}$  CSM, then the problem can be written as  $y_i = x * h_i = Xh_i$ . Further, the



**Figure 1** Left: estimated coil sensitivity for one of 12 coils; Right: estimate normalized by the sum-of-squares of the estimated sensitivities.

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**Figure 2** SENSE reconstructions from the estimated sensitivities on the left and their SoS normalized versions on the right. Red arrow points to a strong artifact.

multichannel convolution can be written as  $Y = XH$ . Thus, if  $x$  has full rank, then the null-space of  $Y$  is equivalent to the null-space of  $H$ . As a result, the null-space (equivalently row-space) vectors used to reconstruct  $y_i$  from subsampled data in PRUNO, can be used for the estimation of  $k$ -space coefficients of CSMs efficiently using the following optimization problem:  $h = \operatorname{argmax}_h ||Vh||^2 + \mu ||Rh||^2$ , where  $R$  represents a low-pass filter, and  $V$  involves convolution matrices of filters obtained from rowspace vectors. For validation, real-time, free-breathing 3-fold cine data were collected on a 3T Siemens scanner with matrix size  $161 \times 144 \times 12 \times 48$ . For CSM estimation, a  $161 \times 24$  fully sampled  $k$ -space was obtained from 3 consecutive time frames. Among 432 singular values, the largest 70 were used as row-space vectors. A Gaussian function was selected for the low-pass  $R$ . The eigenvector associated with the largest eigenvalue of  $V^H V + \mu R^H R$  was calculated to yield the  $8 \times 8$  estimated  $k$ -space coefficients of the CSMs for  $\mu = 5$ . Finally, the sensitivities were normalized with their square-root sum-of-squares (SoS) image.

## Results

Estimated CSM for one coil and its SoS-normalized version are demonstrated in Figure 1. SENSE[4] reconstructions for one of the frames are given in Figure 2 for the estimated CSMs and their SoS-normalized versions. As seen, inhomogeneity and artifacts existing in SENSE reconstruction is significantly reduced with the normalized CSMs. Compared to the image domain processing, the proposed  $k$ -space estimation of CSM was 10 times faster.

## Conclusions

The proposed  $k$ -space approach for CSM estimation using subspace methods and a simple normalization provides both low computational complexity and the flexibility to incorporate both regularization and a low-dimensional parameterization of the smooth CSMs.

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## References

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